

An Influence of Bit Timing Fluctuation in Neuron Spike Trains on M-sequences Detection

Yoshi Nishitani 1) , Chie Hosokawa 2) , Yuko Mizuno-Matsumoto 3) ,
Tomomitsu Miyoshi 1) , Hajime Sawai 1) , Shinichi Tamura 1,4)

1) Graduate School of Medicine, Osaka University, Suita 565-0871, Japan

2) Health Research Institute, National Institute of Advanced Industrial Scientific and Technology (AIST),
Ikeda, Osaka 563-8577, Japan

3) Graduate School of Applied Informatics, University of Hyogo, Kobe 650-0044, Japan

4) NBL Technovator Co. Ltd., 631 Shindachimakino, Sennan 590-0522, Japan

Abstract: In our recent studies, we consider some M-sequences are generated to communicate data in neuronal networks. Then, there is a possibility the tempo of bit timing fluctuate (*tempo fluctuation*) because no mechanism of tempo control of data communication as a clock system of computer is existed in brain.

In this study we analyze the correlation of *margin*, the rate of *tempo fluctuation*, with number of M-sequences from the time course of stimulated action potentials in cultured neuronal networks. Moreover, we tried to analyze the correlation of *margin* with number of M-sequences from simulated neuronal networks and compared with the result from cultured neuronal networks to investigate the reason of *tempo fluctuation*. As results, positive correlations were observed in cultured and simulated neuronal network with *tempo fluctuation*. Meanwhile, no correlation was observed in simulated neuronal network without *clock instability (CI)* which is slippage of clock period. We consider this result suggests that one reason of *tempo fluctuation* was *CI*.

Keywords: Neuron, Spike, Clock Instability, Tempo Fluctuation , M-sequence

1. Introduction

The brain is recognized as a very large-scale network system in which the basic element is a neuron [1-5]. In recent studies of the memory mechanism in the brain, investigating a formation of information communication is more essential than specifying the region of memory in the brain [4].

To investigate what types of memory circuits are assembled and what types of codes are formed to control data communications in brain is essential [6-9].

We analyzed time series patterns of stimulated spike response in cultured neuronal networks [10-13] and detected some pseudo random sequences, especially 0,1 reversed M-sequences [14], above chance in our previous study [15].

In circuit theory, a binary counter with n -bit logical elements (registers) can count up to 2^n-1 . With an adequate feedback link, the loop circuit becomes equivalent to a binary counter, the output of which becomes an M-sequence with length 2^n-1 and is called the period; here, "M" stands for maximum length. If this resulting M-sequence is used as an intrinsic code of its own loop, 2^n-1 loops can be discriminated. For example, a 3-stage linear feedback shift register (LFSR) generates a 7-bits period M-sequence like 1101001 [14].

We consider these results suggest that some equivalent LFSR circuits are assembled and some

M-sequences are generated to communicate data in neuronal networks. Then the question arises as to how tempo (timing) of data communication is controlled in neuronal networks. In computer, tempo of data communication is controlled by exact clock period as shown in Figure 1(a). However, it is possible that *clock instability (CI)* which is slippage of clock period is caused (see Figure 1 (b)) because it seems that no mechanism of tempo control of data communication is existed in brain.

This phenomenon causes interference of sequences. For reasons of as described above, there is a possibility the bit timing fluctuation (*tempo fluctuation*) in sequence. Actually, some *tempo fluctuation* was observed in our previous study [15], however, the detail of generation mechanism of *tempo fluctuation* and the correlation between the magnitude *tempo fluctuation* and number of detected M-sequences are still unclear.

In this study, to investigate these questions, we analyze the correlation of the magnitude *tempo fluctuation* with number of M-sequences from the time course of stimulated action potentials in cultured neuronal networks. Cultured, small-scale neuronal networks on multi-electrode arrays (MEAs) are feasible for analysis of network assemblies. MEAs can be used to apply stimulation pulse into neurons with sufficient flexibility and have been used to identify functional connections in neuronal networks [10-13].

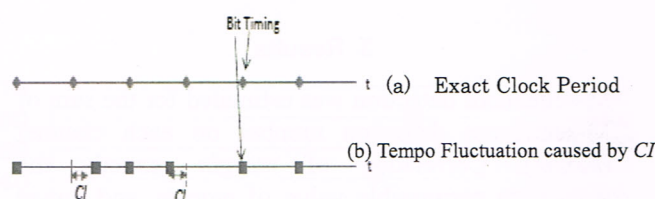


Figure 1 Clock Instability (CI) and Tempo Fluctuation

Now, we summarize definition of terms in this paper.

- Clock Instability (CI) ... Slippage of clock Period
- Tempo Fluctuation ... Bit timing fluctuation in sequence

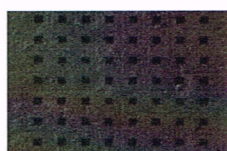
2. Methods

2.1 Cell culture and stimulated spike recording

Cell cultures of hippocampal neurons were dissected from Wistar rats on embryonic day 18. The procedure was performed in accordance with protocols approved by the Institutional Animal Care and Use Committee of AIST. Hippocampi were dissociated with 0.1% trypsin (Invitrogen, Tokyo, Japan) in Ca^{2+} -free and Mg^{2+} -free phosphate-buffered saline minus at 37°C for 15 min. The dissociated neurons were planted at a density of 3.3×10^5 cells/ mm^2 in polyethylentimene-coated MEA dishes (MED-P515A, Alpha MED Scientific, Kadoma, Osaka, Japan) with 8×8 planar microelectrodes. The size of each electrode was $50 \times 50 \mu\text{m}$ and the electrode spacing was $150 \mu\text{m}$. To locate neuronal networks in the central area of each MEA dish, we used a cloning ring with an inner diameter of 7 mm. The ring was removed the following day. Neurons adhered to the substrate of the MEAs covering all electrodes.

Neurons were maintained at 37°C in a humidified atmosphere that contained 5% CO_2 and cultured for 21–40 days in Dulbecco's modified Eagle's medium (Invitrogen) that contained 5% horse serum and 5% fetal calf serum with supplements of 100 U/ml penicillin, 100 $\mu\text{g}/\text{ml}$ streptomycin, and 5 $\mu\text{g}/\text{ml}$ insulin. Half of the culture medium was renewed twice per week. Figure.2 shows a micrograph of cultured neurons in a MEA.

In this study, we prepared 5 cultured cell samples at 22–50 days in vitro (DIV) and named them cultures 1–5



Black rectangles are electrodes. The size of each electrode is $50 \times 50 \mu\text{m}$ and the electrode spacing was $150 \mu\text{m}$.

Figure.2 Micrograph of cultured hippocampal neurons in a MEA

2.2. Stimulated spike recording

Stimulated spikes were recorded by an extracellular recording system with 64 channels (MED64, Alpha MED Scientific). The sampling rate of the recording was 20 kHz and the recording time was 3 s. Stimulation was applied at a particular channel (one electrode) 5 ms after the recording started. Stimulation was produced using a current-controlled bipolar pulse (positive, then negative) with a strength of 10 μA and a duration of 100 μs .

2.3 Detection of M- sequence

M-sequences in stimulated spike responses from cultured neuronal network were detected from raster plot of spike timing the same as [15].

Targets of M-sequences for analyze is shown in table 1. The period of all sequences are 7bits which correspond to period of M-sequences generated from 3 stage LFSR (M3, including Rev.M3 which reverse '0', '1') because only M-sequences whose period were 7bit were detected in [15]. The state was recognized as "1" if a spike existed; otherwise, it was recognized as "0." Then, the raster plot was converted to a time course of binary data in order to investigate sequence patterns. All patterns include 3 or 4 numbers of bit '1'. Considering that the data communication must begin at state "1" because the start of communication could not be identified at state "0," the detection of sequence patterns were started from state "1."

Table 1. Targets of M-sequences for analyze

Pattern No.	Sequence Pattern							
3001	1	1	0	1	0	0	0	Rev. M3
3002	1	0	0	0	1	1	0	Rev. M3
3003	1	0	1	1	0	0	0	Rev. M3
3004	1	1	0	0	0	1	0	Rev. M3
3005	1	0	1	1	1	0	0	
3006	1	1	1	0	0	1	0	
3007	1	1	0	0	1	0	1	
3008	1	0	0	1	0	1	1	
3009	1	1	1	0	1	0	0	
3010	1	0	0	1	1	1	0	
3011	1	1	0	1	0	0	1	
3012	1	0	1	0	0	1	1	

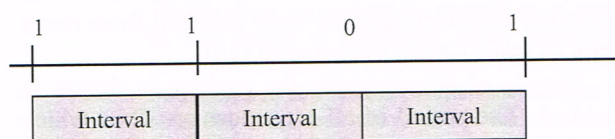
Interval of spikes is disspread variously. So it is crucial to determine the bin size of sequences detection. Some problems of fixed bin always exist [16]. To resolve these problems, the method of

sequences detection was improved as follows.

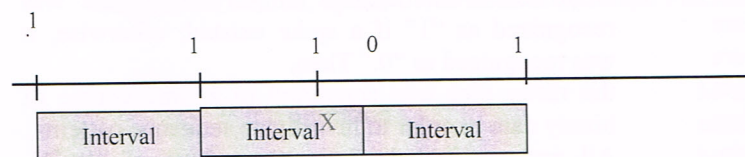
- 1) All spike intervals were detected before detecting sequence patterns.
- 2) The start time of sequence detection was '1'.
- 3) Sequence patterns were scanned with each spike interval with *margin*(see next section).
- 4) If state of '1' was existed in intervals, the detection was recognized fail.

The outline of sequence detection method was shown in Figure 3.

These analyzing programs were implemented by MATLAB.



(a) Detection was succeeded



(b) Detection was failed

Figure 3. Method of sequence detection

2.4 Margin

We called the allowing rate of *tempo fluctuation* when M-sequences were detected was *margin*.

The definition of *margin* was as shown in equation (1) and Figure 4.

$$\text{margin} = \frac{\text{sl}}{\text{interval} \times 6} \times 100 \% \quad \dots (1)$$

Where *sl* corresponds to the slippage of interval and time stamp of state '1' and the denominator of equation (1) equals to the length of detected M-sequence (7bit pattern with 6 intervals).

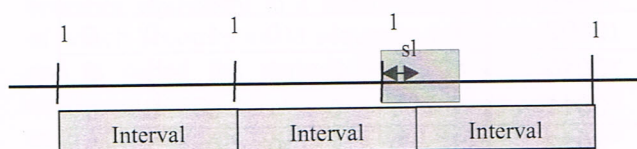


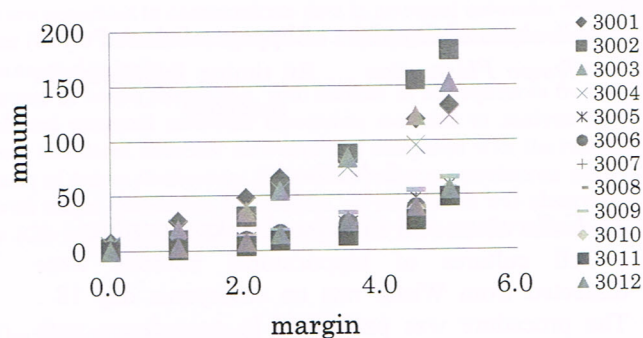
Figure 4. *Margin*

Spike allows to exist in the range indicated sky blue rectangle We detected sequences where the max permissible value of *margin* was 0,1,2,2.5,3.5 and

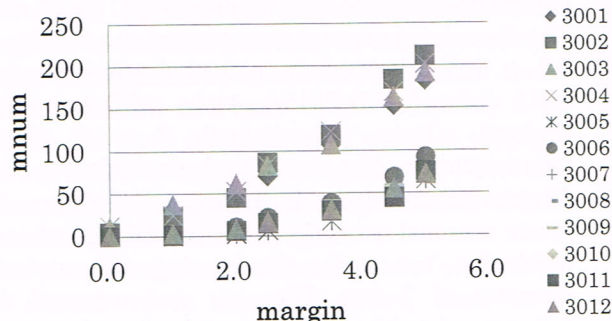
4.5 %.

3. Results

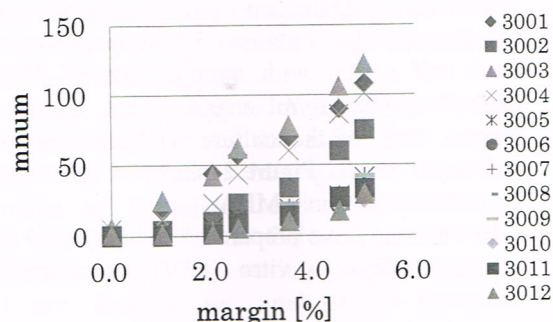
M-sequences detection was estimated for the sum of M-sequences detection number on each channel (*mnum*). Correlation of *margin*, exactly the maximum permissible value of *margin*, and *mnum* of each sequence type was shown in Figure 5. As shown in these figures, positive correlation was observed in all sequence type.



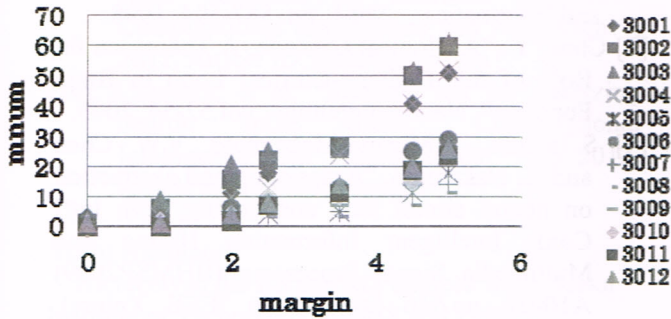
(a) Culture 1



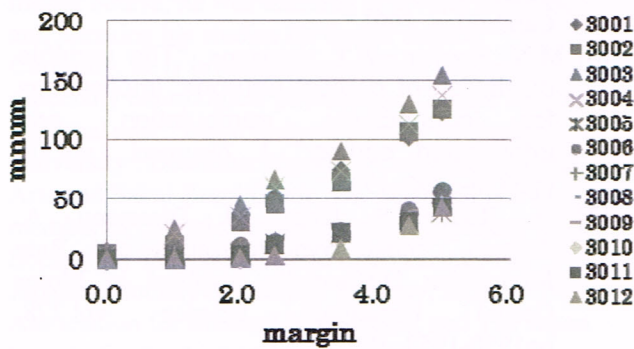
(b) Culture 2



©Culture3



(d) Culture 4



(e) Culture 5

Figure 5 Correlation of *margin* and *mnum*
(Cultured neuronal networks)

4. Discussions

As a analyze result from cultured neuronal networks, the number of detected sequences (*mum*) is influenced by *margin*. This result shows that *tempo fluctuation* exists in sequences. We assume that one reason of *tempo fluctuation* is *CI*. To prove our assumption, we tried to analyze the correlation of *margin* with number of M-sequences from simulated neuronal networks with different *CI* and compared the result with the result from cultured neuronal networks.

Simulated neuronal network was implemented in MATLAB (Math Works Japan. Tokyo, Japan).

The network consists of $n=2000$ neurons. Each neuron is connected excitedly or inhibitedly to all other neurons randomly. *Clock period* of neuron connection control was 0.8ms and 5 type of simulated neuronal networks, the rate of $CI=0\%$, 6%, 12%, 20%, 25%, were implemented. 64 neurons were selected to analyze spike timings similar to recording spike timing of cultured neuronal network on *MED Prob* [13,15].

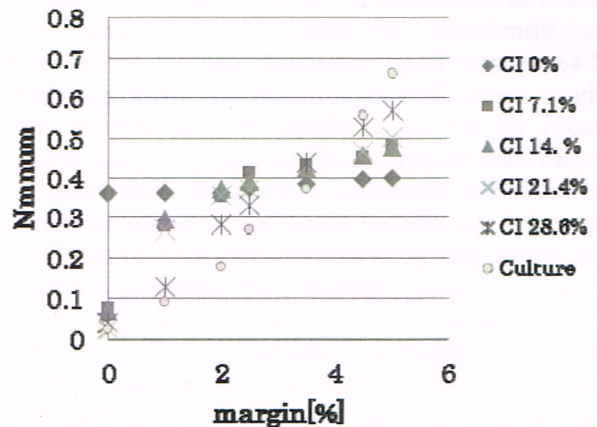
Then, we compared the result with the result from

cultured neuronal networks as follows. First, *mnum* was normalized by equation (2) to allow for neuronal networks (cultured and simulated) with different *mnum* owing to number of spikes, etc.

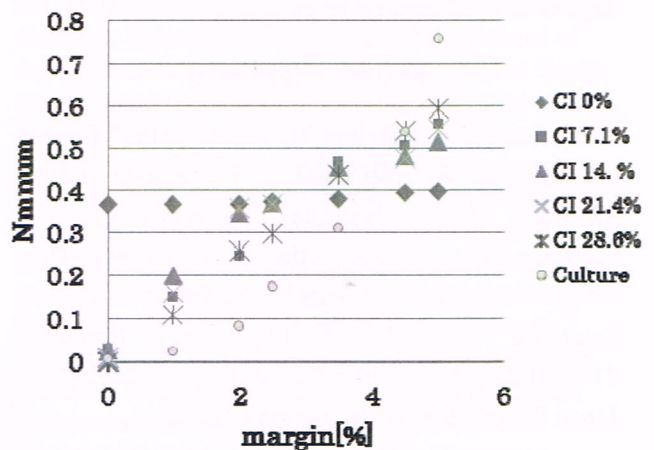
$$Nmnum = \frac{mnum}{\sqrt{\sum_{ma} (mnum_{ma})^2}} \dots (2)$$

Where *Nmnum* is normalized *mnum* and *mnum_{ma}* is sum of detected number of all Rev.M3 (Pattern No.3001-3004) or Non. Rev.M3 (Pattern No.3005-3012, see Table 1) when *margin* = *ma*. Then maximum value of *mnum* was normalized 1.

Next, the correlation of *margin* and normalized sum of *mnum* of all sequence types (*Nmnum*) was analyzed shown in Figure 6.



(a) Rev.M3



(b) Non Rev.M3

Figure 6 Correlation of *margin* and *Nmnum*
Where *Nmnum* of Culture was calculated from mean

mnum of all cultures

As results, when *CI* was 0% (no *tempo fluctuation*), there was no correlation of *mnum* and *margin*.

While, when *tempo fluctuation* was not 0% (with *tempo fluctuation*), there was correlation of *mnum* and *margin* and few numbers of sequences were detected when *margin* was 0% as cultured neuronal networks.

We consider this result suggests that our assumption that one reason of *tempo fluctuation* was *CI* was proved.

5. Conclusion

In this paper, we analyzed the correlation of *margin* with number of M-sequences from the time course of stimulated action potentials in cultured neuronal networks. As results, positive correlation was observed in each culture and *tempo fluctuation* was caused in sequences. Moreover, we tried to analyze the correlation of *margin* with number of M-sequences from simulated neuronal networks whose each *CI* was different to investigate the reason of the *tempo fluctuation*. As results, we proved that one reason of this phenomenon was *CI*. However, the shape of *margin-mnum* correlation of simulated neuronal networks did not so match up to that of cultured neuronal networks even *CI* was not 0%. This suggests that it is possible that other reasons also exist.

Our future work is to do more detail analyze to solve the reason of *tempo fluctuation* more clearly, especially, why the shape of *margin-mnum* correlation of simulated neuronal networks did not so match up to that of cultured neuronal networks.

We consider results of our study are applicable to large section of medical engineering.

Acknowledgements

We thank E. Onishi and M. Suzuki (AIST) for the cell cultures. We also thank Y. Kawaguchi and S. Yabunaka (Osaka Institute of Technology) for supporting the analysis of the spike response. This study was supported in part by the Grant-in-Aid for Scientific Research of Exploratory Research 21656100, and Scientific Research (A) 22246054 of Japan Society for the Promotion of Science.

References

- [1] Bonifazi, P., et al., "GABAergic Hub Neurons Orchestrate Synchrony in Developing Hippocampal Networks," *Science* vol.326, no. 5958. Pp1419-1424, 2009.
- [2] Lecerf, C., "The double loop as a model of a learning neural system. Proceedings World Multiconference on Systemics," *Cybernetics and Informatics*, Vol.1, pp. 587-594, 1998.
- [3] Choe, Y., "Analogical Cascade: A Theory on the Role of the Thalamo-Cortical Loop in Brain Function," *Neurocomputing*, vol.52-54, 2003.
- [4] S.Tamura, Y.Mizuno-Matsumoto, Y.W. Chen and K. Nakamura, "Association and abstraction on neural circuit loop and coding," 5th Int'l Conf. Intelligent Information Hiding and Multimedia Signal Processing (IIHMSP2009) A10-07, no.546 (appears in *IEEE Xplore*). 2009.
- [5] M.Abeles, "Corticonics, Neural Circuits of the Cerebral Cortex," Cambridge University Press, Cambridge, 1991
- [6] M.N. Shadlen, W.T. Newsome, "The variable discharge of cortical neurons: implications for connectivity, computation, and information coding," *J. Neurosci.*, vol.18, pp3870-3896, 1998.
- [7] A. Riehle, S. Grun, M. Diesmann, A. Aertsen, "Spike Synchronization and Rate Modulation Differentially Involved in Motor Cortical Function," *Science* vol.278, pp1950-1953, 1997
- [8] Naoki Masuda and Kazuyuki Aihara, "Dual Coding Hypotheses for Neural Information Representation," *Mathematical Biosciences*, Vol.207, pp.312-321, 2007-6.
- [9] T. Kamimura, et al. "Memory Loop Neural Circuit and Information Communication in Brain," *IEEE. SEDM. Second international conference*. 5.2010.
- [10] P. Bonifazi, M. Elisabetta, and V. Torre, "Static properties of information processing in neuronal networks," *Euro J.Neurosci.* vol.22. 2005.
- [11] P. L. Baljon, M. Chiappalone, and S. Martinoia, "Interaction of electrically evoked responses in networks of dissociated cortical neurons," *Phys Rev E*.80.031906., pp.031906-1 - 031906-10, 2009.
- [12] D. A. Wagenaar, J. Pine, and S. M. Potter. J. "Effective parameters for stimulation of dissociated cultures using multi-electrode arrays," *Neurosci Methods*. 138.pp27-37, 2004.
- [13] C. Hosokawa, et al. "Resynchronization in neuronal network divided by femtosecond laser processing," *Neuroreport*. vol.19, no.7, 2008.
- [14] T.P.Vogels, L.F. Abbott, "Signal propagation and logic gating in networks of integrate-and-fire neurons," *J.Neurosci.*, 25 pp10786-10795, 2005

- [15] Y.Nishitani, C.Hosokawa, Y.Mizuno-Matsumoto, T.Miyoshi, H.Sawai, S.Tamura, "Detection of M-sequences from spike sequence in neuronal networks," Computational Intelligence and Neuroscience, 2012, Article ID, 862579, 9pages
- [16] S.Tamura, et al, "Random bin for analyzing neuron spike trains," Computational Intelligence and Neuroscience, Vol.2012, Article ID 153496, 11pages

Yoshi Nishitani

He received his BS and MS degrees from Osaka Institute of Technology in 1988 and 1990, respectively, and Ph.D in Applied Informatics from University of Hyogo in 2010. After finishing his master course, he was teaching at several colleges, and pursuing his studies for doctor degree. Currently, he is investigating medical engineering, especially neurological physiology, Cardiac Action Potential and hemo dialysis therapy in Osaka University, Doshisha Women's College of Liberal Arts and Sakai Rumi Clinic. Dr. Nishitani is a member of Global Business Society, Japanese Society for Therapeutics and Engineering, The Japanese Society of Dialysis Therapy, Japan Association for Medical Informatics, and The Japan Society for Production Management.

Chie Hosokawa

She received the B.S., M.S., and Ph.D. degrees in applied physics from Osaka University, Osaka, Japan, in 2000, 2002, and 2005, respectively. From 2003 to 2005, she was a research fellow of the Japan Society of Promotion for Sciences. She was a postdoctoral research fellow with the Graduate School of Engineering, Osaka University in 2006. Since Apr. 2006, she has been a researcher in Health National Institute of Advanced Industrial Science and Technology (AIST). Her research interests include neuro-engineering and neuro-photonics, especially laser modulation of network dynamics in dissociated neurons. Dr. Hosokawa is a member of the Japan Society of Applied physics, the Japan Neuroscience Society, and the Society for Neuroscience.

Yuko Mizuno-Matsumoto

She received the M.D. degree from Shiga University of Medical Science, Japan, in 1991, and Ph.D. degrees in Medical Science and Engineering from Osaka University, Japan, in 1996 and 2003, respectively. From 1999 to 2000, she was a Post-Doctoral Research Fellow in the Department of Neurology, Johns Hopkins University, Baltimore, USA. From 2004 to 2011, she was an Associate

Professor, since 2011, she has been a Professor in the Graduate School of Applied Informatics, University of Hyogo, Kobe, Japan. She is a Certifying Physician of The Japanese Society of Psychiatry and Neurology, and a Certifying Physician & Electroencephalographer of Japanese Society of Clinical Neurophysiology.

Tomomitsu Miyoshi

He received the M.D. and Ph.D. degree in Medical Science from Osaka University, Osaka, Japan, in 1993 and 1998, respectively. Since 1998, he has been an Assistant Professor in Graduate School of Medicine, Osaka University. His research interest includes sensory neural processing, neural repair and visual prosthesis.

Hajime Sawai

He obtained his BS degree in human science from Osaka University in 1982. After leaving from Osaka University Graduate School of Medicine, we was with Hirosaki University and afterward also Osaka University as Research Associate. He obtained his Ph.D degree from Graduate School of Medicine of Osaka University in 1992. He became Associate Professor of Okayama Prefectural University in 1994. In 2000, he became Associate Professor, Department of Integrative Physiology, Osaka University Graduate School of Medicine.

Shinichi Tamura

He received the B.S., M.S., and Ph.D. degrees in electrical engineering from Osaka University, Osaka, Japan, in 1966, 1968, and 1971, respectively. He was a Professor of the Graduate School of Medicine, Graduate School of Information Science and Technology, and the Center for Advanced Medical Engineering and Informatics, Osaka University. After retiring from Osaka University in 2007, he joined NBL Co., Ltd, and now with NBL Technovators Co., Ltd as a Director. He has published more than 250 papers in scientific journals and received several awards from journals including Pattern Recognition and Investigative Radiology. He has been working in the field of image analysis and its applications. He is Associate Editor of Pattern Recognition, and Editorial Board member of International Journal of Computer Assisted Radiology and Surgery. Dr. Tamura is IEEE Life Fellow, IEICE Fellow, member of Global Business Society, the Institute of Electronics, Information and Communication Engineers of Japan, the Information Processing Society of Japan, and the Japanese Society of Medical Imaging Technology.